

# ON THE VOLUME FROM PLANAR SECTIONS THROUGH A CURVE

XIMO GUAL-ARNAU

Department of Mathematics, Campus Riu Sec, s/n, University Jaume I, 12071-Castelló, Spain  
e-mail: gual@mat.uji.es  
(Accepted October 19, 2004)

## ABSTRACT

We derive a formula to obtain the volume of a compact domain from planar sections through a curve. From this formula we propose a stereological estimator for the volume which generalizes some known unbiased estimators which use a systematic sampling scheme. Moreover we formulate a Cavalieri's principle for compact domains in spaces of constant curvature  $\lambda$ .

Keywords: Cavalieri, curve, planar sections, space form, unbiased estimator, volume.

## INTRODUCTION

A problem of biomedical interest is how to estimate the volume of an object (bladder, prostate, ...) from planar sections. The best known method to obtain an unbiased estimation of this volume is provided by the Cavalieri's principle, which is based on parallel equidistant plane sections; that is, orthogonal plane sections through a line. The Cavalieri's method has been used for scanning techniques such as computed tomography (Pache *et al.*, 1993) or magnetic resonance imaging (Roberts *et al.*, 1994). However, it is difficult to obtain parallel sections of a given object (organ) by ultrasound scan when such obstacles as bones or air are present between the scanner and the organ. In this case, in Watanabe (1982) the volume of an object in  $\mathbb{R}^3$  is calculated from planar sections through a curve of centroids. From this result, a numerical method has been developed to approximate the volume of an object, whose accuracy has been proved in Treece *et al.* (1999). However, an unbiased estimator of the volume is not available from this method and only from scanning planes which emanate from a common axis, an unbiased estimator for the volume has been derived, based on the ancient theorem of Pappus of Alexandria (Cruz-Orive and Roberts, 1993).

Here we calculate the volume of a compact domain in  $\mathbb{R}^n$  from plane sections through a curve  $c(t)$ . When  $c(t)$  is a line and the plane sections are orthogonal to the curve we obtain the Cavalieri method; when  $c(t)$  is a curve of centroids of the plane sections we obtain the formula in Watanabe (1982) and when  $c(t)$  is a circumference and the plane sections are normal to  $c(t)$ , these plane sections are rotating planes that contain a vertical axis and we have the result in Cruz-Orive and Roberts (1993). Moreover, from this formula we obtain an unbiased estimator for the volume when systematic sampling through the curve is considered.

Stereological estimators of volume, using a systematic sampling scheme, are usually much more precise than those based on independent sampling. Therefore, systematic sampling is widely used in stereology as sampling scheme. Here we will consider systematic sampling through a curve to obtain unbiased estimators for the volume.

Since our principal aim is to present the mathematical foundations to derive formulas to calculate the volume from plane sections through a curve, in section "Volume of domains in  $\mathbb{R}^n$ " we derive the general formula for domains in  $\mathbb{R}^n$  and we obtain some important consequences of this formula. However, in section "Stereological applications" we will concentrate on the applications in volume and area estimation in  $\mathbb{R}^3$  and  $\mathbb{R}^2$ , respectively, and we add two examples of bodies with sectional planes orthogonal to different curves. In section "Discussion" we generalize some results for compact domains in a space form  $M_\lambda^n$  of dimension  $n$  and sectional curvature  $\lambda$ , and we formulate a Cavalieri's principle in  $M_\lambda^n$ .

## VOLUME OF DOMAINS IN $\mathbb{R}^n$

Let  $D$  be a compact domain in the  $n$ -dimensional euclidean space  $\mathbb{R}^n$ . Let  $c : I = [0, L] \rightarrow \mathbb{R}^n$  be a  $C^\infty$  curve parametrized by its arc-length  $t$  ( $c(t)$  may be inside  $D$  or not). For every  $t \in I$ , let  $P_t$  denote a  $(n-1)$ -dimensional plane (hyperplane) in  $\mathbb{R}^n$  through  $c(t)$  (not necessarily orthogonal to  $c(t)$ ). Let  $\{E_1(t), E_2(t), \dots, E_n(t)\}$  be a smooth orthonormal frame along  $c(t)$  such that, for each  $t \in I$ ,  $\{E_2(t), E_3(t), \dots, E_n(t)\}$  is a basis of  $T_{c(t)}P_t \equiv P_t$ .

From now on we will suppose that there exist subsets  $D_t \subset P_t \cap D$  such that

$$D = \bigcup_{t \in I} D_t \quad \text{and} \quad D_{t_1} \cap D_{t_2} = \emptyset \quad \text{for} \quad t_1 \neq t_2. \quad (1)$$

Under the above hypotheses, each point  $x_t \in D_t$  will be given as

$$x_t = c(t) + \sum_{i=2}^n \mu_i(t) E_i(t). \quad (2)$$

Let  $\mu(t) = \sum_{i=2}^n \mu_i(t) E_i(t) = \sum_{i=2}^n \langle \mu(t), E_i(t) \rangle E_i(t)$  and  $N(t) = \mu(t) / |\mu(t)|$ ; then,

$$x_t = c(t) + r_t N(t), \quad (3)$$

where  $r_t = \text{dist}(c(t), x_t)$ .

**Theorem 1.** The volume of  $D$  is given by

$$\begin{aligned} \text{Vol}_n(D) = & \int_0^L \text{Vol}_{n-1}(D_t) \langle c'(t), E_1(t) \rangle dt \\ & - \int_0^L \int_{D_t} r_t \langle N(t), \frac{d}{dt} E_1(t) \rangle \sigma_t dt, \end{aligned} \quad (4)$$

where  $\sigma_t$  is the  $(n-1)$ -dimensional volume element of  $P_t$ .

*Proof.* Let  $\omega$  be the volume element in  $\mathbb{R}^n$  and we consider on  $D$  the coordinates given by  $(t, \mu_2(t), \dots, \mu_n(t))$ ; then,

$$\text{Vol}_n(D) = \int_D \omega = \int_0^L \int_{D_t} \omega(\partial t, E_2(t), \dots, E_n(t)) \sigma_t dt. \quad (5)$$

From the properties of the cross vector product we get

$$\text{Vol}_n(D) = \int_0^L \int_{D_t} \langle \partial t, E_2(t) \wedge \dots \wedge E_n(t) \rangle \sigma_t dt. \quad (6)$$

But

$$\begin{aligned} \partial t = \frac{\partial}{\partial t} \Big|_{x_t} &= \frac{d}{dt} (c(t) + r_t N(t)) \\ &= c'(t) + r_t N'(t), \end{aligned} \quad (7)$$

so

$$\begin{aligned} \langle \partial t, E_2(t) \wedge \dots \wedge E_n(t) \rangle &= \langle \partial t, E_1(t) \rangle \\ &= \langle c'(t), E_1(t) \rangle + r_t \langle N'(t), E_1(t) \rangle \\ &= \langle c'(t), E_1(t) \rangle - r_t \langle N(t), \frac{d}{dt} E_1(t) \rangle. \end{aligned} \quad (8)$$

Now, substituting Eq. 8 in Eq. 6 we obtain the result.

In order to obtain some important consequences of the above theorem we will recall the concept of moment and center of masses of a domain.

## MOMENTS AND CENTER OF MASSES (OR CENTROID) OF $D_t$

Let  $\Gamma$  be a  $(n-2)$ -dimensional plane (that is, an hyperplane in  $P_t$ ) through  $c(t)$ , with unit normal vector field  $\xi$ .  $\Gamma$  separates  $P_t - \Gamma$  into two components. Let  $A$  be the component  $\xi$  points to. Let  $\varepsilon$  be the real function defined on  $P_t$  by

$$\varepsilon(x_t) = \begin{cases} 1 & \text{if } x_t \in A \\ -1 & \text{if } x_t \notin A \end{cases} \quad (9)$$

The moment of  $D_t$  respect to  $\Gamma$  ( $M_\Gamma(D_t)$ ) is given by the integral

$$M_\Gamma(D_t) = \int_{D_t} \varepsilon(x_t) l(x_t) \sigma_t, \quad (10)$$

where  $l$  is the distance from  $x_t$  to  $\Gamma$ .

From elementary trigonometric properties we have that

$$M_\Gamma(D_t) = \int_{D_t} r_t \langle \xi, N(t) \rangle \sigma_t. \quad (11)$$

Hence,  $c(t)$  is the centroid of  $D_t$  if for every unit vector  $\xi \in T_{c(t)} P_t \equiv P_t$ , one has that  $M_\Gamma(D_t) = 0$ .

Now we come back to Theorem 1. Suppose that

$$\frac{d}{dt} E_1(t) = \sum_{i=1}^n a_i(t) E_i(t) \quad (12)$$

and let  $\Gamma_i$  denote the hyperplane orthogonal to  $E_i(t)$  in  $P_t$ , ( $i = 2, 3, \dots, n$ ).

**Corollary 1.** The volume of  $D$  is given by

$$\begin{aligned} \text{Vol}_n(D) = & \int_0^L \text{Vol}_{n-1}(D_t) \langle c'(t), E_1(t) \rangle dt \\ & - \sum_{i=1}^n \int_0^L a_i(t) M_{\Gamma_i}(D_t) dt. \end{aligned} \quad (13)$$

*Proof.* Immediate from (12) and Theorem 1.

Now we will consider some important consequences of the above corollary.

$c(t)$  is a curve of centroids. (See Figs. 1, 2)

Suppose that, for each  $t \in [0, L]$ ,  $c(t)$  is the center of masses of  $D_t$ ; then, from Eq. 13,

$$\text{Vol}_n(D) = \int_0^L \text{Vol}_{n-1}(D_t) \langle c'(t), E_1(t) \rangle dt. \quad (14)$$

The above formula for  $n = 3$  is a generalization of the main result in (Watanabe, 1982); however the method used here to obtain it is completely different.

$P_t$  is orthogonal to  $c$ . (See Figs. 2, 5)

Suppose that for each  $t \in [0, L]$ ,  $P_t$  is an orthogonal hyperplane to  $c(t)$ . Now, we shall consider that the curve  $c(t)$  has a Frenet frame  $\{f_1(t) = c'(t), f_2(t), \dots, f_n(t)\}$ , which is positively oriented and satisfies the Frénet equations:

$$\begin{aligned} f_1'(t) &= k_1(t)f_2(t) \\ f_2'(t) &= -k_1(t)f_1(t) + k_2(t)f_3(t) \\ &\vdots \\ f_{n-1}'(t) &= -k_{n-2}(t)f_{n-2}(t) + k_{n-1}(t)f_n(t) \\ f_n'(t) &= -k_{n-1}(t)f_{n-1}(t), \end{aligned} \tag{15}$$

where  $k_i(t)$  is called the  $i$ th curvature of  $c(t)$ .

Then, from Corollary 1, substituting  $E_1(t)$  by  $f_1(t)$  we obtain

$$\begin{aligned} Vol_n(D) &= \int_0^L Vol_{n-1}(D_t) dt - \\ &\int_0^L k_1(t) M_{\Gamma_2}(D_t) dt, \end{aligned} \tag{16}$$

where  $M_{\Gamma_2}(D_t)$  is the moment of  $D_t$  respect to the hyperplane in  $P_t$  orthogonal to  $f_2(t)$ .

**Corollary 2.** When  $c(t)$  is a straight line in  $\mathbb{R}^n$ , ( $k_i(t) = 0$ ), or when  $M_{\Gamma_2}(D_t) = 0$ , we obtain the Cavalieri's formula

$$Vol_n(D) = \int_0^L Vol_{n-1}(D_t) dt. \tag{17}$$

From Eq. 9 and Eq. 10, if  $D_t^+ = D_t \cap A$  and  $D_t^- = \{x_t \in D_t / x_t \notin A\}$ , we have that  $M_{\Gamma_2}(D_t) = 0$  means

$$\int_{D_t^+} l(x_t) \sigma_t = \int_{D_t^-} l(x_t) \sigma_t, \tag{18}$$

that is, the distance from the centroid of  $D_t^-$  to  $\Gamma_2$  and the distance from the centroid of  $D_t^+$  to  $\Gamma_2$  coincide.

## STEREOLOGICAL APPLICATIONS

In this section we will concentrate on the stereological applications of volume estimation in  $\mathbb{R}^3$  and area estimation in  $\mathbb{R}^2$ .

Let  $D$  be a compact domain in  $\mathbb{R}^3$  and  $c(t)$  a curve which satisfy the conditions imposed in Eq. 1 and such that  $P_t$  is the orthogonal plane to  $c(t)$ . We define

$$f(t) = Area(D_t) - k(t)M_2(D_t), \tag{19}$$

where  $k(t)$  is the curvature of  $c(t)$  and  $M_2(D_t)$  is the moment of  $D_t$  with respect to the line in  $P_t$  given by the binormal vector of the Frenet frame in  $c(t)$ .

Then,  $Vol(D)$  can be expressed as an integral  $Vol(D) = \int_0^L f(t) dt$  and may be estimated from systematic sampling on  $[0, L]$ ; that is, let  $T = L/m$  and  $t_0$  a point placed uniformly at random in  $[0, T]$ , then

$$\widehat{V}(t_0) = T \sum_{i=0}^{m-1} f(t_0 + iT) \tag{20}$$

is an unbiased estimator of  $Vol(D)$ .

Since  $c$  is parametrized by its arc -length it is locally injective. If we suppose that  $c$  is globally injective ( $c$  has no self-intersections), then  $c$  is an isometry and therefore the distance between  $c(t_0 + iT)$  and  $c(t_0 + (i - 1)T)$  is  $T$ ; that is, the sets  $D_{iT}$  are orthogonal to the curve and placed at equidistant intervals with spacing  $T$  along the curve. Moreover, the point  $\alpha(t_0)$  is placed uniformly at random in  $[\alpha(0), \alpha(T)]$ .

It is important to note that the torsion of  $c$  does not appear in Eq. 20. Properties of this kind of estimators (variance, etc.) have been widely considered in the literature (see, e.g., Gual-Arnau and Cruz-Orive (1998)).

Note that when  $c(t)$  is a curve of centroids or when  $c(t)$  is a line ( $k(t) = 0$ ) the measure function  $f(t)$  is given by  $f(t) = Area(D_t)$ .

For a compact domain  $D$  in  $\mathbb{R}^2$ ,  $f(t)$  has the form

$$f(t) = Length(D_t) - k(t)M_{c(t)}(D_t), \tag{21}$$

with

$$M_{c(t)}(D_t) = \int_{D_t} \varepsilon(x_t) r_t \eta_t, \tag{22}$$

where  $\eta_t$  is the line element of  $P_t$  and  $\varepsilon(x_t)$  is given by Eq. 9.

Now we will prove that the method developed in Eq. 3.3 of Cruz-Orive and Roberts (1993), to obtain the volume of a domain in  $\mathbb{R}^3$  from scanning planes which emanate from a common axis  $Oz$ , is a particular case of our method when the curve  $c(t)$  is a circumference of unit radius placed in a plane orthogonal to  $Oz$ .

Using the notation in Cruz-Orive and Roberts (1993) and supposing that  $D_t$  lies entirely in the half space  $A$ , the moment  $M_{\Gamma_2}(D_t)$  can be written as:

$$M_2(D_t) = -l_1^+(t) Area(D_t), \tag{23}$$

where  $l_1^+(t)$  is the distance from  $\Gamma_2$  to the centroid of  $D_t$ . Then, from Eq. 21 and Eq. 23, we have

$$\begin{aligned} Vol(D) &= \int_0^{2\pi} Area(D_t)dt + \int_0^{2\pi} l_1^+(t)Area(D_t)dt \\ &= \int_0^{2\pi} Area(D_t)(1 + l_1^+(t))dt = \int_0^{2\pi} l_2^+(t)Area(D_t)dt, \end{aligned} \tag{24}$$

where  $l_2^+(t)$  is the distance from  $Oz$  to the centroid of  $D_t$ , which is the Eq. 3.3 in Cruz-Orive and Roberts (1993).

To finish this section we will present two examples with schematic figures of different domains, curves and planes sections.

In the first example the curve  $c(t)$  is a curve of centroids which is inside  $D$ .

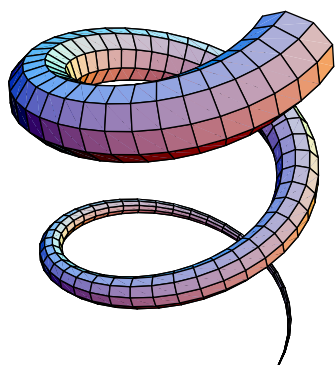


Fig. 1. *Domain D.*

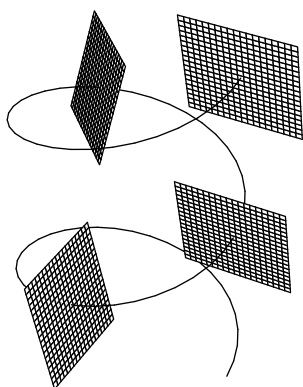


Fig. 2. *Curve of centroids and portions of planes  $P_t$  orthogonal to the curve.*

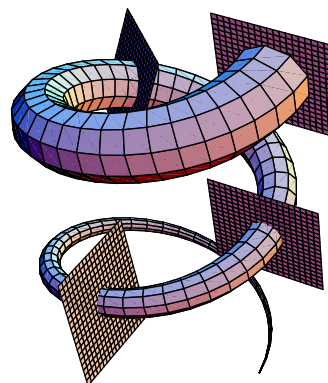


Fig. 3. *Domain with some plane sections which give  $D_t$ .*

In the second example the curve  $c(t)$  is outside  $D$  and the scheme is similar to that of Cavalieri.

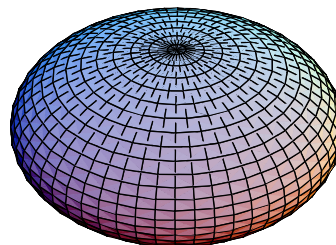


Fig. 4. *Domain D.*

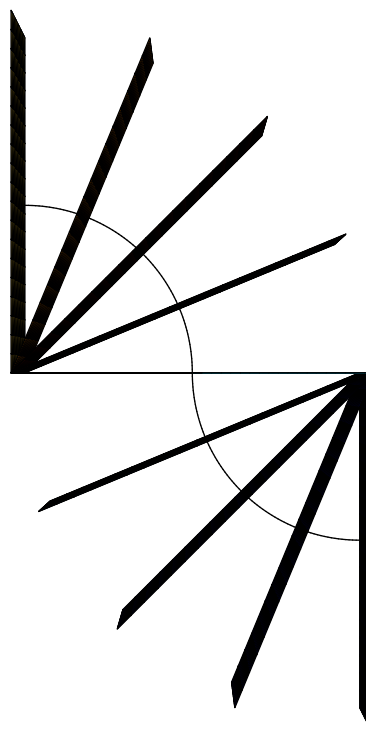


Fig. 5. *Curve  $c(t)$  and planes  $P_t$  vertical to the  $x-y$  plane.*

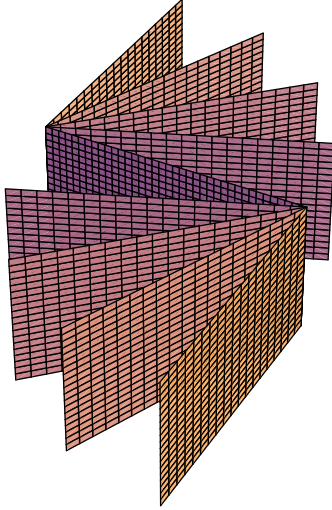


Fig. 6. Planes  $P_t$  from another viewpoint.

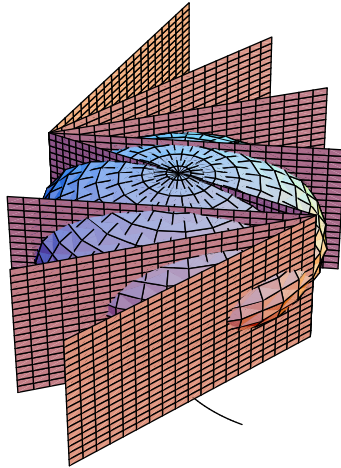


Fig. 7. Domain with some plane sections and the curve  $c(t)$ .

## DISCUSSION

Stereological estimators of volume using a systematic scheme, based on equidistant cuts through a line, are usually much more precise than those based on independent sampling; because any systematic sample represents the whole material better than most samples obtained by independent sampling. Our estimator Eq. 20 preserves the systematic sampling scheme and offers the possibility to choose an alternative curve to a line whose orthogonal sample planes represent better the whole material.

On the other hand, our approach may be adapted to several clinical areas; for example, in the vessel study from IVUS (Intravascular Ultrasound) images, an artery can be modelled as a tube of non-constant

section (Fig. 3 is a particular case of these tubes), where the catheter trajectory is the curve  $c$ .

When the measurement function  $f(t)$  given in Eq. 19 is not known, its estimation will depend on the information provided in each practical case.

## VOLUME OF DOMAINS IN A SPACE FORM

Now we will extend Eq. 16 for compact domains  $D$  in a simply connected space form  $M_\lambda^n$  of dimension  $n$  and sectional curvature  $\lambda$ , with  $\lambda \neq 0$  (for  $\lambda = 0$  we have the results in Section 2). Let  $c : I = [0, L] \rightarrow M_\lambda^n$  be a  $C^\infty$  curve parametrized by its arc-length  $t$  and, for every  $t \in [0, L]$ , let  $P_t$  denote a complete totally geodesic hypersurface of  $M_\lambda^n$  through  $c(t)$  and orthogonal to the curve  $c$ . We suppose that there exists a Frenet frame along  $c$  with the same properties as in Eq. 15 but  $f'_i(t)$  means, now, the covariant derivative of  $f_i(t)$  along  $c(t)$ ,  $\left(\frac{\nabla}{dt} f_i(t)\right)$ .

Under the same assumptions as in Eq. 1, each point  $x_t \in D$  will be given by

$$x_t = \exp_{c(t)} r_t N(t) = \exp_{c(t)} \mu(t), \quad (25)$$

where

$$\mu(t) = \sum_{i=2}^n \mu_i(t) F_i(t). \quad (26)$$

Supposing now that  $D \subset U$ , where  $U$  is the image by  $\exp$  of an open set of the normal bundle of  $c$  on which  $\exp$  is a diffeomorphism, we may consider on  $U$  the coordinates:

$$\phi(\exp_{c(t)} r_t N(t)) = (t, \mu_2(t), \dots, \mu_n(t)), \quad (27)$$

then

$$\text{Vol}_n(D) = \int_0^L \int_{D_t} \langle \partial t, \tau_r f_2(t) \wedge \dots \wedge \tau_r f_n(t) \rangle \sigma_t dt, \quad (28)$$

where  $\tau_r$  is the parallel transport from  $c(t)$  to  $\gamma_{N(t)}(r_t)$  ( $\gamma_{N(t)}$  is the geodesic with  $\gamma_{N(t)}(0) = c(t)$  and  $\gamma'_{N(t)}(0) = N(t)$ ).

Now,

$$\partial t = \frac{d}{dt}(\exp_{c(t)} r_t N(t)) = Y_1(r_t), \quad (29)$$

where  $Y_1$  is the Jacobi field along  $\gamma_{N(t)}$  satisfying:

$$Y_1(0) = f_1(t), \quad Y'_1(0) = \frac{\nabla}{dt} N(t), \quad (30)$$

which is given by Gray and Miquel (2000)

$$Y_1(r_t) = c_\lambda(r_t) \tau_r f_1(t) + s_\lambda(r_t) \tau_r \frac{\nabla}{dt} N(t), \quad (31)$$

where, for every  $\lambda \in \mathbb{R}$ ,  $s_\lambda : \mathbb{R} \rightarrow \mathbb{R}$  will denote the solution of the equation  $s'' + \lambda s = 0$  with the initial conditions  $s(0) = 0$  and  $s'(0) = 1$ ; and  $c_\lambda = s'_\lambda$ ; i. e.

$$s_\lambda(s) = \begin{cases} \sin(s\sqrt{\lambda})/\sqrt{\lambda}, & \lambda > 0 \\ s, & \lambda = 0 \\ \sinh(s\sqrt{\lambda})/\sqrt{\lambda}, & \lambda < 0. \end{cases} \quad (32)$$

(Note that for  $\lambda = 0$ ,  $Y_1(r_t)$  is given by Eq. 7).

Finally, from Eq. 28 and Eq. 31 we have that

$$\begin{aligned} Vol_n(D) &= \int_0^L \left( \int_{D_t} c_\lambda(r) \sigma_t \right) dt \\ &\quad + \int_0^L \int_{D_t} s_\lambda(r_t) \left\langle \frac{\nabla}{dt} N(t), f_1(t) \right\rangle \sigma_t dt \\ &= \int_0^L \left( \int_{D_t} c_\lambda(r) \sigma_t \right) dt - \int_0^L M_{\Gamma_2}(D_t) k_1(t) dt, \end{aligned} \quad (33)$$

where

$$M_{\Gamma_2}(D_t) = \int_{D_t} s_\lambda(r_t) \langle f_2(t), N(t) \rangle \sigma_t, \quad (34)$$

and Eq. 33 generalizes Eq. 16 for space forms  $M_\lambda^n$ .

In the particular case where the compact domain  $D$  is obtained by a motion of a domain  $D_0$  through the curve  $c(t)$ ; Eq. 33 has been obtained in Gray and Miquel (2000).

## ABOUT THE CAVALIERI PRINCIPLE

### IN $M_\lambda^n$

The Cavalieri principle, already familiar to the ancient Greeks, states that the volumes of two solids in  $\mathbb{R}^n$  are equal if the areas of the corresponding sections drawn perpendicular to a straight line are equal. This principle is not valid when totally geodesic hypersurfaces perpendicular to a given geodesic are considered; however, from Eq. 33 it is possible to formulate this principle for compact domains in  $M_\lambda^n$  as follows:

*Volumes of two compact domains in  $M_\lambda^n$  are equal if the integrals*

$$\int_{D_t} c_\lambda(r) \sigma_t \quad (35)$$

*are equal through a geodesic  $c(t)$  in  $M_\lambda^n$  where  $r$  denotes the geodesic distance from  $x$  to  $c(t)$ .*

(The integral Eq. 35 is equal to  $Vol_{n-1}(D_t)$  for  $\lambda = 0$  and it is called the ‘modified volume’ in Choe and Gulliver (1992).)

## ACKNOWLEDGEMENTS

The research was supported by the grant BSA2001-0803-C02-02. The author wishes to thank to the referees for helpful suggestions.

## REFERENCES

- Cruz-Orive LM, Roberts N (1993). Unbiased volume estimation with coaxial sections: an application to the human bladder. *J Microsc* 170:25-33.
- Choe J, Gulliver R (1992). Isoperimetric inequalities on minimal submanifolds of space forms. *Manuscripta Math* 77:169-89.
- Gray A, Miquel V (2000). Pappus type theorems on the volume in space forms. *Ann Glob Anal Geom* 18:241-54.
- Gual-Arnau X, Cruz-Orive LM (1998). Variance prediction under systematic sampling with geometric probes. *Adv Appl Probab (SGSA)* 30:889-903.
- Pache J C, Roberts N, Vock P, Zimmermann A, Cruz-Orive LM (1993). Vertical LM sectioning and parallel CT scanning designs for stereology: application to human lung. *J Microsc* 170:9-24.
- Roberts N, Garden AS, Cruz-Orive LM, Whitehouse GH, Edwards RHT (1994). Estimating of fetal volume by magnetic resonance imaging and stereology. *Brit J Radiol.* 67:1067-77.
- Treece G, Prager R, Gee A, Berman L (1999). Fast surface and volume estimation from non-parallel cross-sections, for freehand three-dimensional ultrasound. *Med Image Anal* 3:141-73.
- Watanabe Y (1982). A method for volume estimation by using vector areas and centroids of serial cross sections. *IEEE Trans Biomed Eng* 29:202-5.